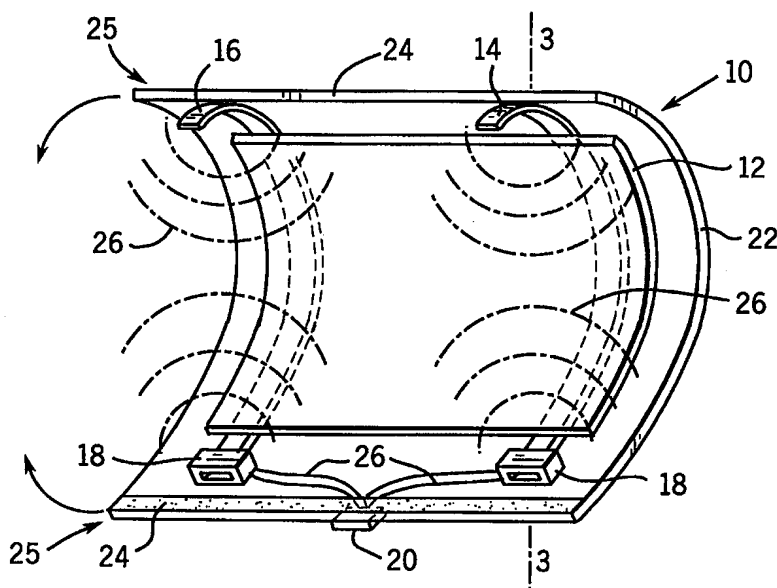




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(54) Title: CONDUCTANCE MEASURING APPARATUS



(57) Abstract

A conductance sensor uses an auto-tuning oscillator to drive a coil inducing eddy currents in a substance to be measured. The auto-tuning oscillator precisely controls the amplitude of oscillations to eliminate amplitude-dependent effects. The coil may be used to sense the presence of a conducting fluid in a nonconducting pipe or the proximity of a metallic object to the coil. The coil may be used in a cardiac or respiratory monitor having a fixed loop conductor. Monitoring changes in the conductivity of a subject provides a measure of cardiac or respiratory motion.

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CONDUCTANCE MEASURING APPARATUS

Field of the Invention

The present invention relates to a sensor for measuring conductance of material and in particular a sensor that may be used, among other applications, for measuring periodic
5 respiratory and cardiac motion by detecting changes in the conductance of patient tissue.

Background of the Invention

Conductance Measurement

The conductance of a material, that is, how well it
10 conducts electricity, may be determined by applying a voltage to the material with a pair of electrodes and measuring the corresponding current flow.

This approach, while straightforward, has several disadvantages. First, it is sensitive to localized high
15 resistances at the interface between the electrodes and the material. Second, the electrodes used to apply the voltage must contact the material raising issues of contamination of the materials and corrosion of the electrodes.

For this reason, it is known to make non-contacting
20 measurement of conductivity using a pair of electrical coils immersed in the material being measured. The premise behind such systems is that electrical coupling of an alternating current signal between the two coils is functionally related to the conductivity of the material between the coils. Such
25 systems have the disadvantage of requiring multiple coils.

A single coil resistivity measuring system (resistivity being the inverse of conductivity) is described in U.S. Patent 4,536,713. In this system, eddy currents are induced in a

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drilling fluid for an oil well or the like by a magnetic field applied via a ferrite core. The measured eddy currents, as reflected on the driving voltage of the coil, provide a coarse indication of drilling liquid resistivity.

5 Respiration Monitoring

Electronic monitoring of respiration may be performed for critically ill or comatose patients, small children at risk of sudden infant death ("SID"), or patients with sleep apneas (partial suspension of breathing sometimes associated with
10 insomnia).

There are two types of sleep apnea. Obstructive apnea, is caused by blockage of the windpipe or mouth and nose, and is characterized by a change in the phase relationship between respiratory movement of the chest and abdomen. In central
15 apnea, the patient ceases all signs of breathing.

Distinguishing central apnea from obstructive apnea requires independent detection of abdominal and thoracic respiratory motion.

A number of different types of respiration sensors are
20 known in the art, including mechanical sensors employing air flow measuring turbines or the like, that require the use of a face mask or mouthpiece, and inflatable cuffs which measure chest or abdomen extension manifest as a change in cuff pressure. Such mechanical systems can suffer from problems of
25 reliability.

Respiratory motion may be also detected electronically by conductive coils wrapped around the patient. In one prior art device, multiple inductive coils are positioned on the patient to move with respect to each other as the patient breathes.
30 The mutual inductance between the coils changes with their relative motion and is measured to detect respiratory motion.

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In a somewhat different design, respiratory deformation of a single coil causes a change of inductance in that coil which may be measured by the detuning of an oscillator using the coil's inductance as a tuning element. The change in
5 frequency of the oscillator is used as a measure of respiratory motion.

With these electrical sensors, the sensing coil must be snugly fit to the patient so as to move with the patient and for this reason may create an unpleasant confining sensation
10 or pressure on the patient's trunk and stomach. Such constraining pressure is particularly problematic with small infants. Such electronic sensors are unsuitable for measuring cardiac motion which does not result in significant distention of the patient's chest or abdomen.

15 **Summary of the Invention**

The present invention provides a single-coil non-contacting conductance sensor that provides improved accuracy in conductance measurement. By driving the single coil at its resonant frequency (as coupled to the measured material),
20 capacitive and inductive effects are minimized making the eddy current measurement more robust against the influence of the geometry of the measurement and qualities of the material other than its conductance.

Specifically, the sensor includes a conductive coil
25 driven by an auto-tuning oscillator. The auto-tuning oscillator seeks a resonant frequency of the conductance coil as coupled to a measured material and its environment to induce eddy currents in the measured material. An impedance measuring circuit is connected to the conductive coil
30 providing a measure of the effective resistance of the coil at the resonant frequency as reflects the magnitude of the

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induced eddy currents within the sample.

Thus, it is another object of the invention to provide a simplified conductance measuring sensor that is resistant to inductive and capacitive effects. By driving the coil at its
5 natural resonant frequency, the resistive effects to be measured dominate.

The auto-tuning oscillator may include a gain controlled amplifier having a gain control input signal reflecting the amplitude of the signal driving the coil, and the impedance
10 measuring circuit, may derive resistance from the gain control signal.

Thus it is another object of the invention to provide a conductance sensor that is resistant to amplitude dependent effects in the conductance measuring process.

15 The gain control signal may be provided by a synchronous rectifier, rectifying an oscillator signal from the oscillating current synchronously with the oscillating current. The synchronous rectifier may be a multiplier multiplying the oscillator signal by itself.

20 Thus it is another object of the invention to provide a conductance sensor that is resistant to asynchronous noise sources. The synchronous rectifier is not switched by larger amplitude out-of-phase or different frequency signals which will then be averaged out in a subsequent filtering stage.

25 One application of the conductance sensor is electronic monitoring of respiratory (or cardiac) motion which relies on the measurement of changes in conductivity in the patient's tissue within a limited cross-sectional area. Because the measurement does not rely on changes in the coil's dimensions,
30 the sensor may be less constraining to the patient and more robust against deformation of the coil in use.

Specifically, the conductive coil is sized to fit about

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the body of a person. The auto-tuning oscillator, connected to the conductive coil, drives the coil with an oscillating current at a resonant frequency to induce eddy currents in the person. Attached to the conductive coil is the impedance measuring circuit which provides a measure of the effective resistance of the coil at the first frequency as reflects the magnitude of the induced eddy currents within the person. An electronic filter receiving this impedance signal extracts a periodic plethysmographic signal.

Thus, it is one object of the invention to provide a method of measuring periodic physiological motion, such as cardiac or respiratory motion, by detecting changes in areal conductance of patient tissue within a coil without the need to deform the coil in time with the physiological motion. Because the invention does not require outward distention of the patient, it is equally effective to measure periodic internal conductance changes, for example those caused by the heartbeat, as with those conductance changes which are reflected in outward movement of the patient, such as breathing.

The patient monitor may include two coils sized to fit about the body of the person, one in the abdominal area of the person and one in the thoracic area of the patient. Here, the impedance measuring circuit provides measures of the effective resistance of the two coils separately. An alarm may compare these separate resistance measurements to determine when distress of the person is indicated.

Thus, it is another object of the invention to provide an electronic respiratory detector that can provide separate measures of two different regions of the body in proximity to each other. Because only a single coil is needed to measure conductivity, multiple measurements may be made by adjacent

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multiple coils.

The foregoing and other objects and advantages of the invention will appear from the following description. In the description, reference is made to the accompanying drawings which form a part hereof and in which there is shown by way of illustration, a preferred embodiment of the invention. Such embodiment does not necessarily represent the full scope of the invention, however, and reference must be made therefore to the claims herein for interpreting the scope of the invention.

Brief Description of the Drawings

Figure 1 is a perspective view of a belt incorporating the present invention and shown in position on an infant;

Figure 2 is a perspective view of the belt of Figure 1 when open showing the localization of the magnetic fields from two coils in the abdominal and thoracic region;

Figure 3 is a plot of magnetic field strength versus distance along line 3-3 of Figure 2 when the belt is closed;

Figure 4 is a schematic diagram of a circuit used to drive the coils of Figure 2 and to provide a conductance measurement of the region of the magnetic fields shown in Figure 2;

Figure 5 is a block diagram showing subsequent processing of the conductance measurement; and

Figure 6 is a perspective view of a general-purpose conductance sensor employing the principle of the present invention.

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DETAILED DESCRIPTION OF THE PREFERRED EMBODIMENT

Belt Construction and Loop Placement

Referring to Figure 1, the present invention may be incorporated into a belt 10 for wrapping about the trunk of a patient 12, such as an infant, with the upper edge of the belt being positioned about the patient's thoracic region and the lower edge of the belt being positioned about the patient's abdomen.

Referring also to Figure 2, the belt 10 may include an inner fabric sleeve 12 providing electrical insulation and cushioning to the patient 12 against various rigid portions of the belt 10 as will be described.

Attached to the outside of the sleeve 12 near the superior and inferior edges of the belt 10 are first and second flexible electrical conductors 14 and 16 which open into a C-shaped form when the belt 10 is opened. Connectors 18, attached to one end of each of conductors 14 and 16, physically join together the ends of conductors 14 and 16, to form two loops, one about the thoracic and one about the abdominal regions of the patient 12 when the belt 10 is closed, as shown in Figure 1. The opposing ends of each of the conductors 14 and 16 remain electrically isolated so that an oscillating electrical signal may be applied across the ends of conductor 14 and conductor 16.

The conductors 14 and 16 may be flat metal springs of a conductive material such as brass so as to open and close without permanent deformation.

An outer insulating fabric sleeve 22 covers the inner sleeve 12, sandwiching the conductors 14 and 16 between the inner sleeve 12 and the outer sleeve 22. Medial edges 25 of the outer sleeve 22 support opposite halves of a strip

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fastener 24, such as Velcro, so that the medial edges 25 may be removably attached to one another to close the belt 10 about the patient 12 and to resist outward forces which might serve to disconnect conductors 14 and 16 from connectors 18.

5 Additional circuitry 20 which includes two oscillators, to be described below, and a low powered radio transmitter to transmit signals from the patient 12, and a battery is connected to each of the connectors 18 and thus to both ends of each conductor 14 and 16 by wires 26 running along the
10 inner surface of the outer sleeve 22 and passing through the outer sleeve 22 to the circuitry 20.

Conductivity Measurement with Eddy Currents

Referring now also to Figure 3, when the conductors 14 and 16 are formed into a loop with a closing of the belt about
15 the patient 12, alternating current passing through the conductors 14 and 16 generates oscillating magnetic fields 26 within the patient 12. Figure 3 shows the amplitude of magnetic fields along a transverse plane through the patient caused by current flow through conductors 14 and 16.

20 As shown in Figure 3, the amplitude of the magnetic field A is concentrated within the patient 12 and of relatively low magnitude outside of the patient, the boundaries of which are indicated by vertical lines 30. The strength of the magnetic field falls off rapidly in a direction perpendicular to the
25 plane of the coils of the conductors 14 and 16 and thus interference in the measurements obtained by the coils 14 and 16 is low.

The oscillating magnetic fields 26 will induce eddy currents within the patient 12, the magnitude of which are
30 proportional to the conductivity of the tissue. For example, if the tissue of the patient 12 were perfectly conductive, the

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eddy currents would be sufficient to generate a magnetic field (back EMF) opposing the magnetic field 26 to perfectly cancel that magnetic field 26. On the other hand, to the extent that the tissue of the patient 12 is not perfectly conductive, the eddy fields will be lower, and the magnetic field 26 will be reduced but not canceled. Thus, a measurement of the back EMF created by the eddy currents within the patient provides an indication of the conductivity of the patient tissue.

Referring now to Figure 4, the effective circuit of a conductor 14 or 16 in proximity to the patient 12 may be modeled as a first inductor L1 (comprised of either conductor 14 or conductor 16), inductively coupled (as if in a transformer) to a second inductor L2, connected in series with a resistance R_2 . The inductor L2 and resistance R_2 are not discrete elements, but are the equivalent lumped values incorporating the distributed inductance and resistance of many looping current paths of the eddy currents through tissue of the patient 12. Generally, however, R_2 will reflect a total conductivity ($1/R$) in the region within a given loop 14 and 16.

Relationship Between Conductivity And Physiological Motion

This resistance R_2 in turn will depend generally on the real resistance, (W/cm^2), of the tissue in the area enclosed by the loop 14 or 16 times the area enclosed by the loop 14 or 16. For this reason, changes in the cross-sectional area of the patient 12 within either loop 14 or 16 will produce changes in the value of R_2 measured with that loop 14 or 16.

Further, changes in the cross-sectional area of an organ within the patient 12 and within the plane of a loop 14 or 16, and having a noticeably different areal resistance than the

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surrounding tissue will also be reflected in a change in the value of R_2 . For this reason, the value of R_2 will show both respiratory motion in which the patient's overall cross-sectional area changes, and cardiac motion in which a relative
5 area of highly conductive blood changes within the patient without significant overall change in the overall patient cross-sectional area.

Resistance Measuring Circuitry

The value of R_2 is detectable as a decrease in the
10 quality factor of an oscillator employing conductor 14 or 16 as an inductive component of an oscillator tank circuit. The oscillator is formed from the parallel combination of inductance L_1 being one of conductor 16 or 14, and a capacitor C_1 contained within the electronics circuitry 20. In a
15 preferred embodiment, C_1 is selected to tune the combination of L_1 and C_1 into parallel resonance at approximately 4.5 MHz. For conductors 14 and 16 formed into a loop having a diameter of approximately 100 millimeters, C_1 will be a capacitor of 330 pF.

20 As is known in the art, the quality factor of an oscillator provides a measure generally indicating how long an oscillator would continue to oscillate without the input of additional energy (free oscillation). Without eddy currents, the oscillator formed of conductors 14 or 16 would be expected
25 to oscillate for a time limited only by the intrinsic resistance of the conductors 14 and 16 and the other components forming the oscillating resonant circuit. With eddy currents, the resulting back EMF adds an effective power dissipating resistance to the oscillator, shortening the time
30 of free oscillation. Thus, a measure of the quality factor of oscillators formed from conductors 14 and 16 provides an

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indication of the conductivity of the patient 12.

The measurement the of quality factor of a resonant circuit is well known in the art. However, in the present invention, an extremely precise measurement is required and
5 the measurement must be robust in the environment of a moving patient and in a situation where the value of L_1 may change from measurement-to-measurement based on some inadvertent deformation of the conductors 14 and 16, and in variations of attaching the belt 10 to the patient 12.

10 In order to improve the quality factor measurement, the measurement is made at the resonant frequency of the parallel combination of C_1 and L_1 . In fact, the oscillator driving the loops 14 and 16 effectively tracks to the resonant frequency of the parallel combination of C_1 and L_1 as will be described.
15 Thus the effect of variations in the resonant frequency of L_1 and C_1 with respect to the oscillator frequency, such as might effect the quality factor measurement, is reduced. It will be further understood that by driving the coil at resonant frequency, undesired capacitive and inductive influences on
20 the measurement are reduced because the inductive components of the detected signal will cancel the capacitive components of that signal.

In addition, the amplitude of the oscillator driving the parallel combination of L_1 and C_1 is precisely controlled to a
25 constant value. Thus, the effect of amplitude on the quality factor measurement is eliminated and apparent changes in quality factors such as might be caused by a slight detuning of the oscillator with respect to the inductive parallel combination of L_1 and C_1 , are reduced.

30 In a preferred embodiment, an oscillator providing the desired feature of tracking the resonance of C_1 and L_1 and providing a constant amplitude oscillation is provided through

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the use of an operational transconductance amplifier (OTA) 32 connected at its output 38 to one junction between capacitor C_1 and inductor L_1 . The remaining junction between C_1 and L_1 is connected to ground.

5 As is understood in the art, an operational transconductance amplifier provides a current at its output 38 that may be modeled as a gain factor G_m times the voltage across inverting and non-inverting inputs 36 (indicated by a minus and plus sign, respectively) of the operational
10 transconductance amplifier 32. The value G_m is determined by an amplifier bias current I_{abc} .

 The output 38 of the OTA 32 is also connected to the non-inverting input 36 of the OTA 32. In this positive feedback configuration, the output current of the OTA 32 will naturally
15 oscillate at the resonant frequency of the parallel combination of C_1 and L_1 to produce an oscillator signal 41.

 This oscillator signal 41 on output 38 is also received by an amplitude detector 40 which is a precision synchronous rectifier and low-pass filter providing a DC voltage
20 proportional to the amplitude of the oscillator signal 41 at output 38. The synchronous rectifier is realized in the preferred embodiment by a multiplier that accepts at its two factor inputs the output 38. Any noise signal on output 38 that is asynchronous with the oscillator signal 41 will
25 average to zero in the low pass filter. The output of the amplitude detector 42 is received by an inverting input of a standard high-gain operational amplifier 42, whose positive input receives a precision reference voltage 44 designated as V_r .

30 The amplifier 42 operates open-loop, and hence it will be understood that if the voltage on the inverting input of the amplifier 42 is greater than V_r , the output of amplifier 42

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will be a negative value. On the other hand, if the voltage on the inverting input of the amplifier 42 is negative with respect to V_r , the output of amplifier 42 will be positive. The output of the amplifier 42, termed V_{out} , is applied to
5 limiting resistor 43 to become amplifier bias current I_{abc} .

The connection of the output of the amplifier 40 to the OTA 32 provides feedback control of the amplitude of the oscillator signal 41 to the value of V_r . As connected in this manner, the value of V_{out} being the amplitude error signal
10 indicates generally how much additional energy must be input into the oscillator of C_1 and L_1 to maintain oscillation at the desired amplitude of V_r and thus provides a measure of the quality factor of the oscillator of C_1 and L_1 and hence a measure of R_2 . Generally, the higher the value of V_{out} , the
15 less the value of R_2 .

Referring now to Figure 5, the circuit of Figure 4 is repeated once for each of the conductors 14 and 16 and hence two values of V_{out} will be obtained, each indicating the conductivity of the patient within the area encircled by
20 respective loops 14 and 16. These two signals distinguished as V_{out2} (referring to the signal from coil 16 and from the abdomen) and V_{out1} (referring to the signal from coil 14 and from the thoracic region), are each received by separate low-pass filters 50 and 52, respectively, which are tuned to
25 reject the fundamental frequency of the oscillator signal 42 driving the loops 14 and 16, but to pass lower frequency signals caused by a slowly varying change in the value of R_2 with respiration or cardiac motion. In the following discussion, it will be assumed that the frequency of the
30 low-pass filters 50 and 52 is adjusted to extract respiratory motion such as may be needed to diagnose sleep apnea.

The signals from the low-pass filters 50 and 52 are then

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provided to a low-powered radio transmitter 54 contained within the circuitry 20 shown with respect to Figure 2. A nearby receiver 56 receiving this signal extracts two respiratory signals. The transmitter and receiver circuits 54 and 56 are constructed according to techniques well-known in the art, and may be a simple low-power FM link with a different frequency assigned to each of the different respiratory signals.

The receiver 54 provides the respiratory signals to a detector and alarm circuit 58 which is programmed to detect patient distress. The detector and alarm circuit 58 may provide an alarm indicating a loss of respiratory signal extending for more than a certain period of time.

Alternatively, or in addition, the alarm and detector circuit 58 may detect a loss of phase coherence between the signals V_{out1} and V_{out2} such as may indicate obstructive apnea as described before. The detector and alarm 58, in a preferred embodiment, are a microprocessor programmed to receive digitized samples of the respiratory signals and to monitor them according to the criteria described above or other criteria that may be selected by a physician.

It will be recognized that this approach of detecting cardiac and respiratory signals through a measurement of changes in conductivity does not require that the loops 14 and 16 be deformed or flexed with motion of the patient 12, and in fact, the circuit would work if loops 14 and 16 were perfectly rigid and unyielding. As a result, the patient 12 is not unduly compressed about the torso by pressure by the belt 10 other than that minimally necessary to hold the belt 10 in position.

Referring now to Figure 6, the above-described circuit may also find use in measuring the conductivity of an

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arbitrary material, such as a liquid 58 passing through a pipe 60. Here a single conductor 14 is used passing in one or more loops about the circumference of the tube 60 so as to again generate an internal oscillating magnetic field (not shown) inside the tube 60. The back EMF of the eddy currents so induced is detected by measuring the quality factor of an oscillator formed of the conductor and a parallel capacitor (not shown) as described above.

Unlike other conductance sensors in the prior art, no direct contact is required between the liquid 58 and one or more electrodes of the circuit, nor is it necessary that the loop 14 be immersed in the liquid 58 such as may produce clogging or unnecessary turbulence, or that the loop 14 be used in conjunction with a second loop 16.

The measurement of conductivity in this manner may provide an indication of the composition of the liquid 58 and may detect inclusions such as air bubbles or the like.

The liquid 58 need not fill the tube 60, however. To the extent that the liquid 58 occupies only a portion of the cross-sectional area excited by the coil 14, the conductivity will look proportionately lower.

Many other modifications and variations of the preferred embodiment which will still be within the spirit and scope of the invention will be apparent to those with ordinary skill in the art. For example, the conductance probe may be used over a large volume and thus as a means of detecting the presence of people in a room. On a smaller scale the conductance sensor may be used to detect nearby high or low conductance materials including metal and thus function as a proximity switch. In order to apprise the public of the various embodiments that may fall within the scope of the invention, the following claims are made.

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CLAIMS

We claim:

1. A conductivity sensor comprising
a conductive coil;
5 an auto-tuning oscillator connected to the conductive coil to drive the coil with an oscillating current at a resonant frequency of the conductance coil as coupled to a measured material and its environment to induce eddy currents in the measured material; and
10 an impedance measuring circuit connected to the conductive coil providing a measure of the effective resistance of the coil at the resonant frequency as reflects the magnitude of the induced eddy currents within the sample.
2. The conductivity sensor of claim 1 wherein the auto-
15 tuning oscillator is an amplifier having an output connected to the coil and configured for positive feedback.
3. The conductivity sensor of claim 1 wherein the auto-tuning oscillator includes a gain controlled amplifier having a gain control input signal reflecting the amplitude of the
20 signal driving the coil; and
wherein the impedance measuring circuit derives resistance from the gain control signal.
4. The conductivity sensor of claim 3 wherein the gain control signal is provided by a synchronous rectifier,
25 rectifying an oscillator signal from the oscillating current synchronously with the oscillating current.

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5. The conductivity sensor of claim 4 wherein a synchronous rectifier is a multiplier multiplying the oscillating signal by itself.

6. The conductivity sensor of claim 1 including a guide
5 for positioning the measured material in a predetermined relationship with respect to the coil.

7. The conductivity sensor of claim 1 wherein the guide is a non-conductive tube through which a liquid may pass.

8. The conductivity sensor of claim 1 wherein the
10 sample is proximate but outside the coil.

9. A patient monitor comprising:

at least one conductive coil sized to fit about a body of a person;

an auto-tuning oscillator connected to the conductive
15 coil to drive the coil with an oscillating current at a resonant frequency of the conductance coil as coupled to a measured material and its environment to induce eddy currents in the person;

an impedance measuring circuit connected to the
20 conductive coil providing a measure of the effective resistance of the coil at the resonant frequency as reflects the magnitude of the induced eddy currents within the person; and

an electronic filter receiving the measure of impedance
25 to extract a periodic plethysmographic signal.

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10. The patient monitor of claim 9 wherein the filter provides a periodic plethysmographic signal indicating respiration by the person.

11. The patient monitor of claim 9 wherein the filter
5 provides a periodic plethysmographic signal indicating the patient's heartbeat.

12. The patient monitor of claim 9 including in addition, a conductive shield surrounding the coil on the side of the coil away from the person.

10 13. The patient monitor of claim 9 including an alarm circuit monitoring the periodic plethysmographic signal to produce an alarm signal when distress of the person is indicated.

14. The patient monitor of claim 9 having two conductive
15 coils sized to fit about the body of the person, one in an abdominal area of the person and one in a thoracic area of the patient wherein the impedance measuring circuit provides measures of the effective resistance of the two coils separately; and

20 wherein the alarm circuit compares these separate resistance measures to determine when distress of the person is indicated.

15. The patient monitor of claim 9 wherein the auto-tuning oscillator is an amplifier having an output connected
25 to the coil and configured for positive feedback.

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16. The patient monitor of claim 9 wherein the auto-tuning oscillator includes a gain controlled amplifier having a gain control signal reflecting the amplitude of the signal driving the coil; and

5 wherein the impedance measuring circuit derives resistance from the gain control signal.

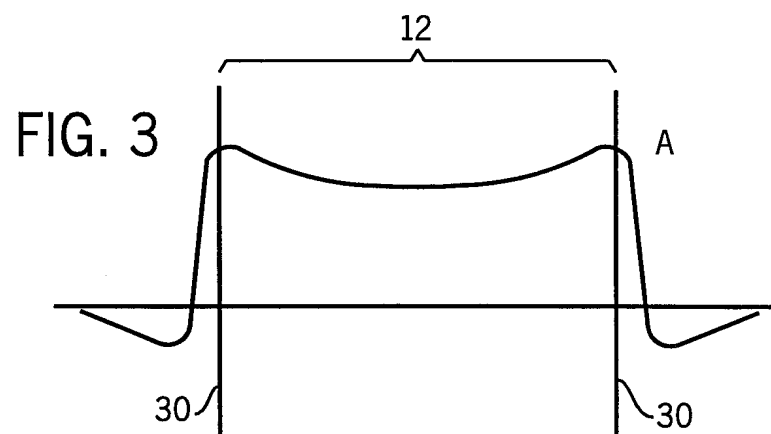
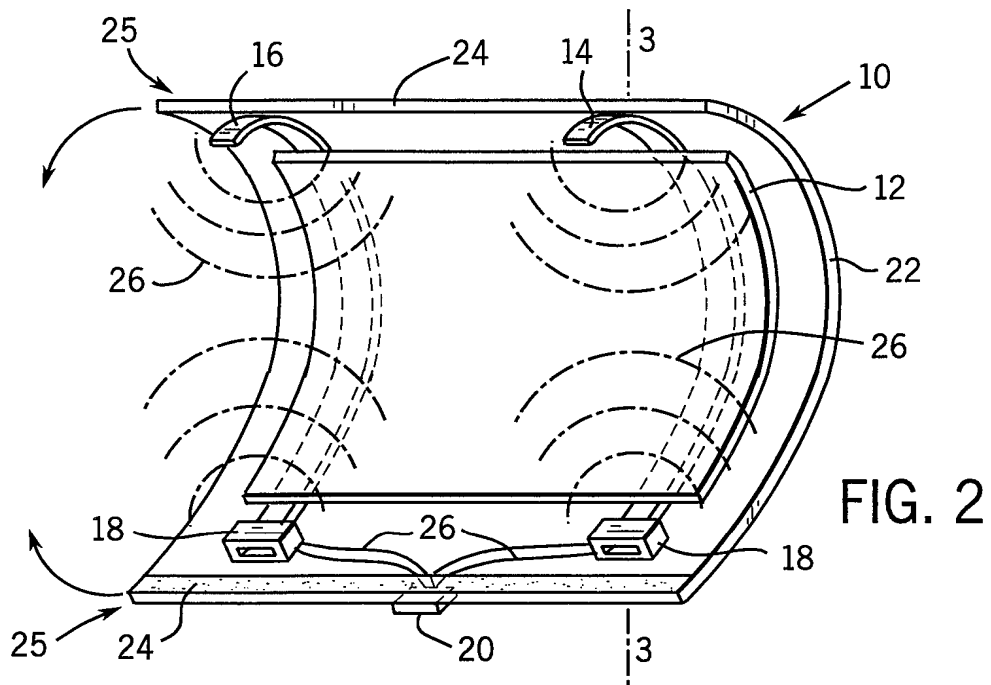
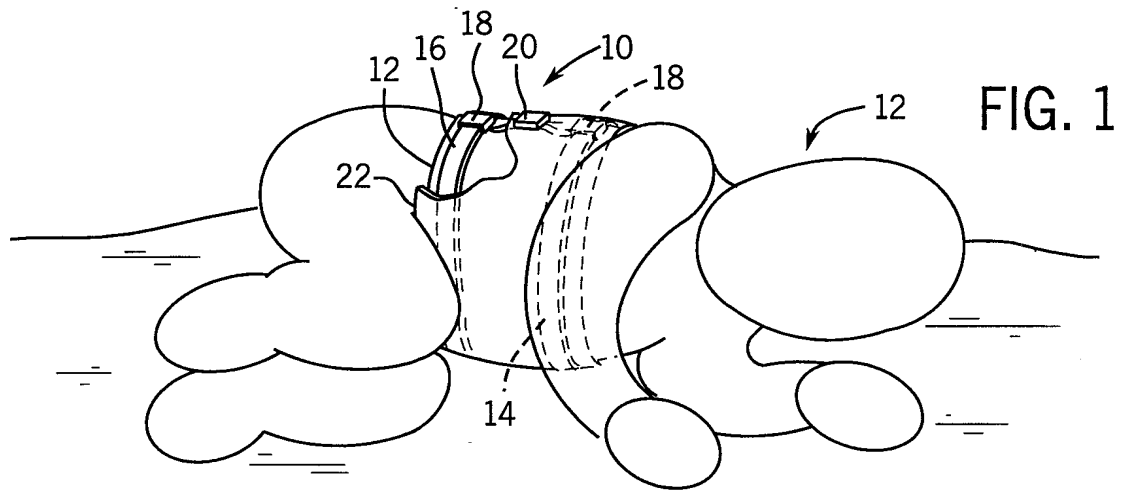
17. A patient monitoring belt comprising
a fabric inner sleeve sized to fit about the body of a person;

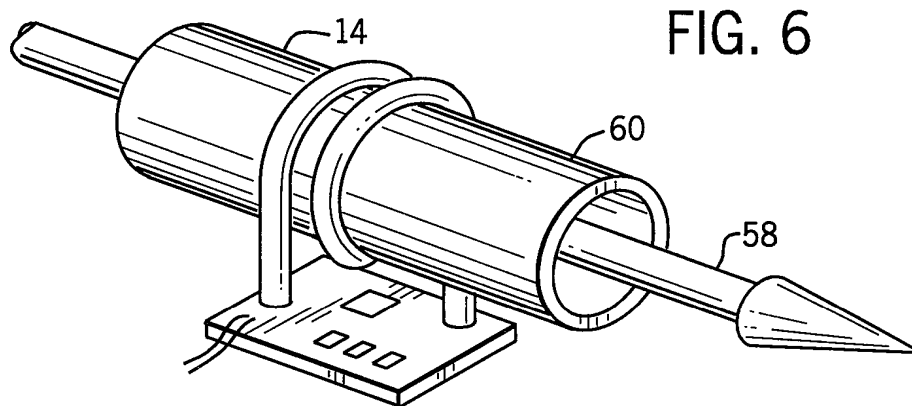
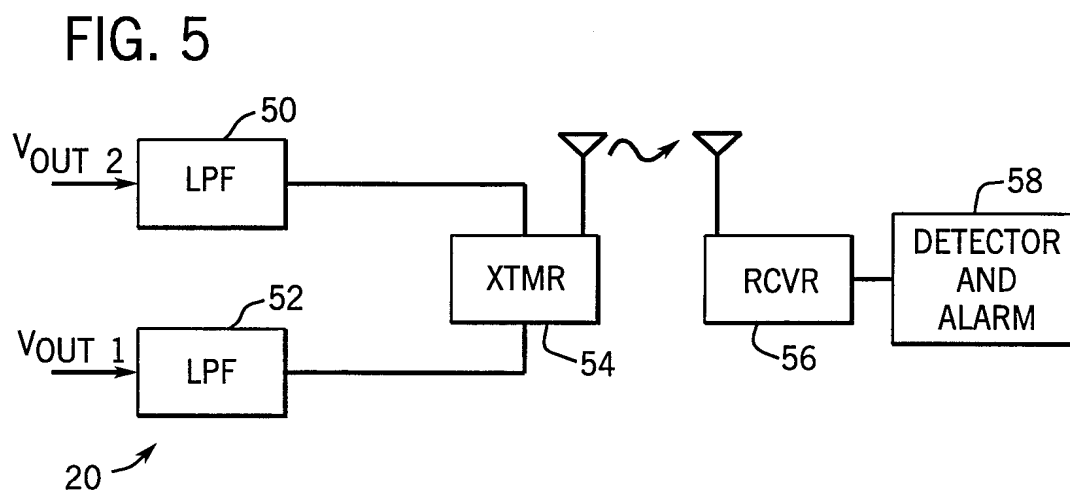
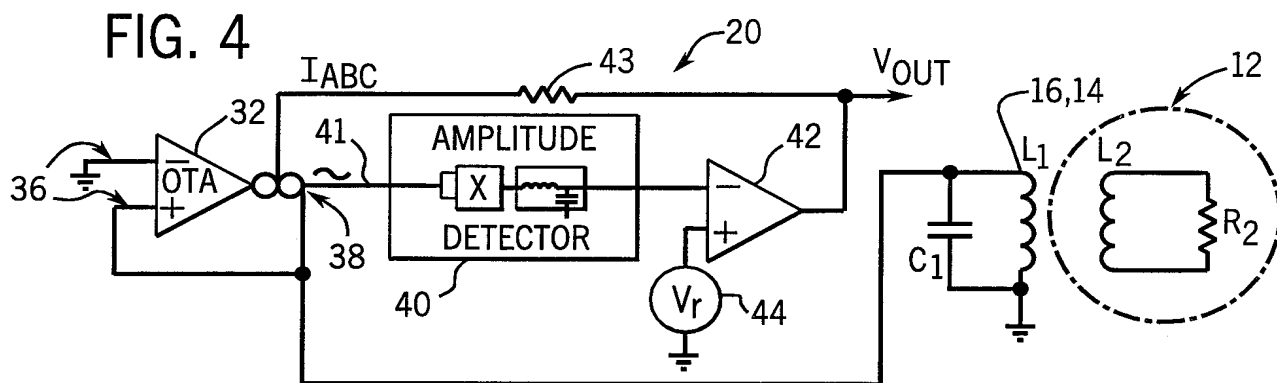
10 a first and second coil positioned circumstantially around the sleeve in spaced apart relationship to fit one in an abdominal region and the other in a thoracic region of the patient when the sleeve is in place on the patient;

15 a first and second auto-tuning oscillator for exciting the first and second coils into resonance; and

an impedance measuring circuit providing a measure of the resistance of the first and second coils at resonance.

18. The patient monitoring belt of claim 17 including a conductive outer sleeve fitting coaxially around the outside
20 of the first and second coil and the inner sleeve._





INTERNATIONAL SEARCH REPORT

Int .ional Application No

PCT/US 97/17897

A. CLASSIFICATION OF SUBJECT MATTER

IPC 6 A61B5/113

According to International Patent Classification (IPC) or to both national classification and IPC

B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)

IPC 6 A61B

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practical, search terms used)

C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category °	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X	US 5 291 782 A (H.E. TAYLOR) 8 March 1994 see column 1, line 61 - column 2, line 28 see column 3, line 26 - column 4, line 56 ---	1,2,6,8
Y	US 4 279 257 A (P.A. HOCHSTEIN) 21 July 1981	1
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Further documents are listed in the continuation of box C.



Patent family members are listed in annex.

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Date of the actual completion of the international search

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INTERNATIONAL SEARCH REPORT

Int. Application No
PCT/US 97/17897

C.(Continuation) DOCUMENTS CONSIDERED TO BE RELEVANT

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